

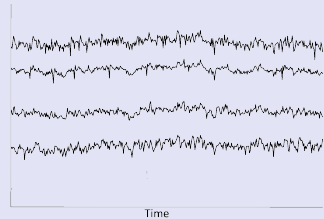
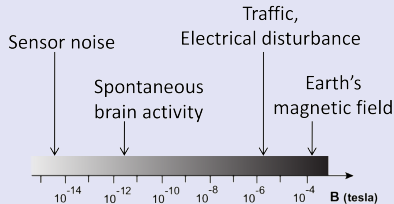
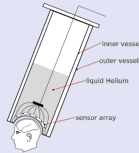
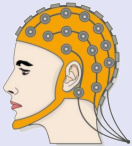
Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals

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INRIA Saclay



Studying brain activity through electromagnetic signals

- ▶ Brain (electrical) activity produces an electromagnetic field.
- ▶ This can be measured with EEG or MEG.



Goal: Study Oscillation in Neural Data

Oscillations are believed to play an important role in cognitive functions.

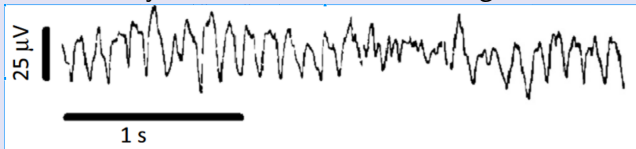
Many studies rely on Fourier or wavelet analyses:

- ▶ Easy interpretation,
- ▶ Standard analysis e.g. canonical bands alpha, beta or theta.

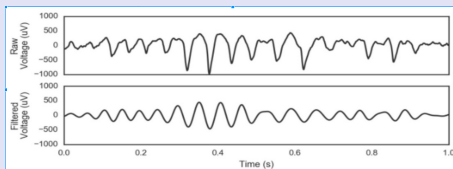
[Buzsáki, 2006]

Goal: Study Oscillation in Neural Data

However, some brain rhythms are not sinusoidal, e.g. mu-waves [Hari, 2006]



and filtering degrades waveforms

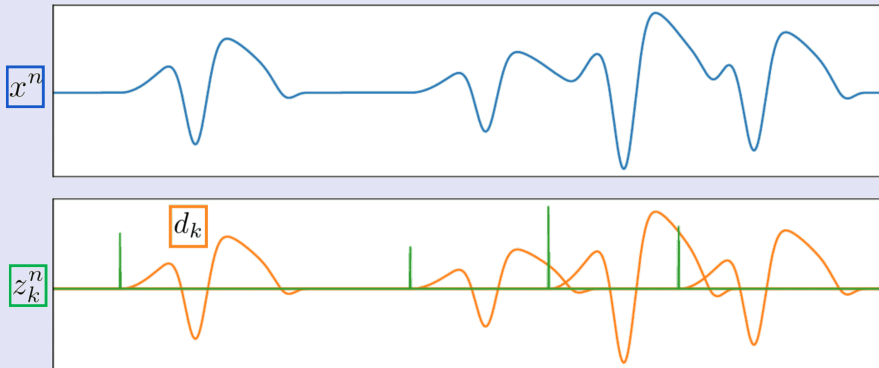


The shape of the waveform can be linked to the information flow between neurons.

⇒ Can extract them with an unsupervised data-driven approach?

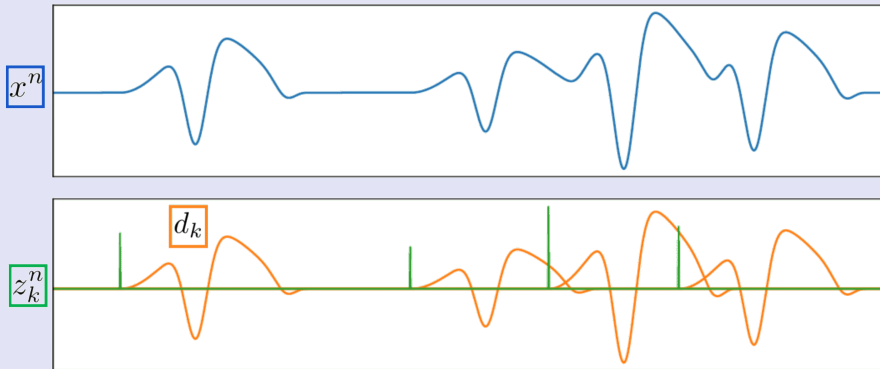
Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape



Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape

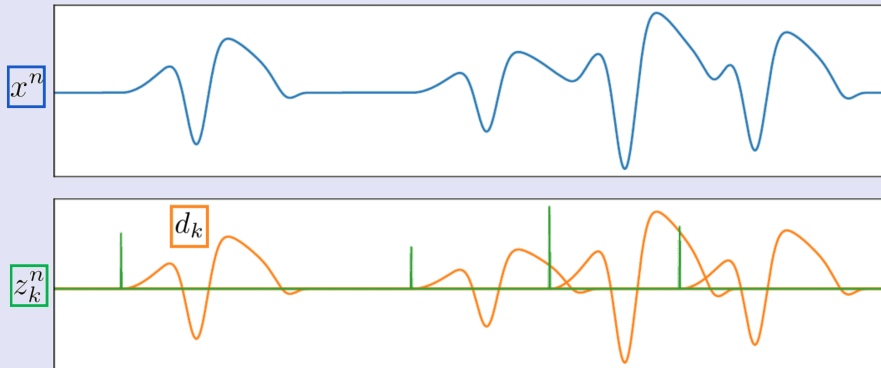


**Convolutional
Representation:**

$$x^n[t] = \sum_{k=1}^K (z_k^n * d_k)[t] + \varepsilon[t]$$

Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape



**Convolutional
Dictionary Learning:**

$$\begin{aligned} \min_{d, z} \quad & \sum_{n=1}^N \frac{1}{2} \left\| \boxed{x^n} - \sum_{k=1}^K \boxed{z_k^n} * \boxed{d_k} \right\|_2^2 + \lambda \sum_{k=1}^K \|\boxed{z_k^n}\|_1, \\ \text{s.t.} \quad & \|\boxed{d_k}\|_2^2 \leq 1 \end{aligned}$$

Shift-invariant Patterns in images



Images also have shift-invariant patterns that we might want to detect.

Convolutional Dictionary Learning (CDL)

[Grosse et al., 2007]

For a set of N univariate signals x^n , solve

$$\min_{d_k, z_k^n} \sum_{n=1}^N \frac{1}{2} \|x^n - \sum_{k=1}^K z_k^n * d_k\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1 \quad (1)$$

Hypothesis: patterns d_k are not present everywhere in the signal. They are localized in time.

\Rightarrow Sparse activation signals z

Extra hypothesis: the patterns are in the ℓ_2 -ball: $\|d_k\|_2^2 \leq 1$.

Bi-convex: The problem is not jointly convex in z_k^n , and d_k but it is convex in each block of coordinate.

Alternate minimization (*a.k.a.* Bloc Coordinate Descent):

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal X^n .
- ▶ **D-step:** given a fixed estimate of the activation, update the atoms in the dictionary d_k .

Rank-1 constrained dictionary learning

References

- ▶ Dupré la Tour, T., Moreau, T., Jas, M., and Gramfort, A. (2018).
Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals.
In *Advances in Neural Information Processing Systems (NeurIPS)*, pages
3296–3306, Montreal, Canada

How to extend CSC to multivariate signals?

We can just use multivariate convolution,

$$\underbrace{X[t]}_{\in \mathbb{R}^P} = \sum_{k=1}^K (z_k * D_k)[t] = \sum_{k=1}^K \sum_{\tau=1}^L z_k[t - \tau] \underbrace{D_k[\tau]}_{\in \mathbb{R}^P}$$

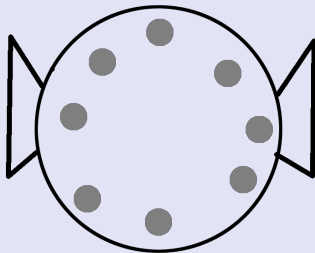
with:

- ▶ X a multivariate signal of length T in \mathbb{R}^P
- ▶ D_k a multivariate signal of length L in \mathbb{R}^P
- ▶ z_k a univariate activation signal of length $\tilde{T} = T - L + 1$

However, this model does not account for the physics of the problem.

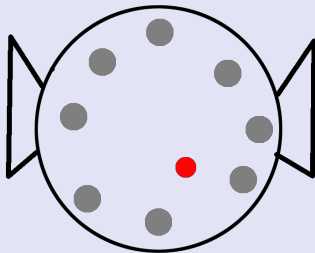
EM wave diffusion

- ▶ Recording here with 8 sensors



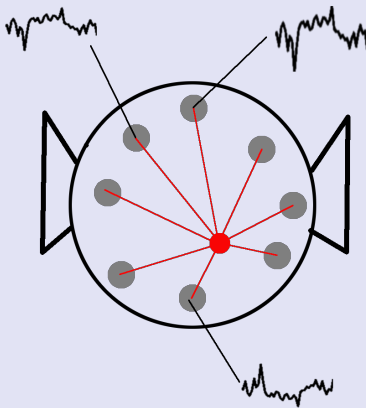
EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain



EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain
- ▶ The electric field is spread **linearly** and **instantaneously** over all sensors (Maxwell equations)



Multivariate CSC with rank-1 constraint

Idea: Impose a rank-1 constraint on the dictionary atoms D_k

To make the problem tractable, we decided to use auxiliary variables u_k and v_k s.t. $D_k = u_k v_k^\top$.

$$\begin{aligned} \min_{u_k, v_k, z_k^n} \quad & \sum_{n=1}^N \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top) \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1, \\ \text{s.t.} \quad & \|u_k\|_2^2 \leq 1, \|v_k\|_2^2 \leq 1 \text{ and } z_k^n \geq 0. \end{aligned} \quad (2)$$

Here,

- ▶ $u_k \in \mathbb{R}^P$ is the spatial pattern of our atom
- ▶ $v_k \in \mathbb{R}^L$ is the temporal pattern of our atom

Tri-convex: The problem is not jointly convex in z_k^n , u_k and v_k but it is convex in each block of coordinate.

We can use a block coordinate descent, aka alternate minimization, to converge to a local minima of this problem. The 3 following steps are applied alternatively:

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal X^n .
- ▶ **u-step:** given a fixed estimate of the activation and temporal pattern, update the spatial pattern u_k .
- ▶ **v-step:** given a fixed estimate of the activation and spatial pattern, update the temporal pattern v_k .

Z-step: Locally greedy coordinate descent (LGCD)

N independent problem such that

$$\min_{z_k^n \geq 0} \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * D_k \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1.$$

This problem is convex in z_k and can be solved with different techniques:

- ▶ Greedy CD [Kavukcuoglu et al., 2010]
- ▶ Fista [Chalasani et al., 2013]
- ▶ ADMM [Bristow et al., 2013]
- ▶ L-BFGS [Jas et al., 2017]

⇒ These methods can be slow for long signals as the complexity of each iteration is at least linear in the length of the signal.

Z-step: Locally greedy coordinate descent (LGCD)

For the Greedy Coordinate Descent, only 1 coordinate is updated at each iteration: [\[Kavukcuoglu et al., 2010\]](#)

1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.

$$z'_k[t] = \max \left(\frac{\beta_k[t] - \lambda}{\|D_k\|_2^2}, 0 \right),$$

$$\text{with } \beta_k[t] = \left[D_k^\top * \left(X - \sum_{l=1}^K z_l * D_l + z_k[t] e_t * D_k \right) \right] [t]$$

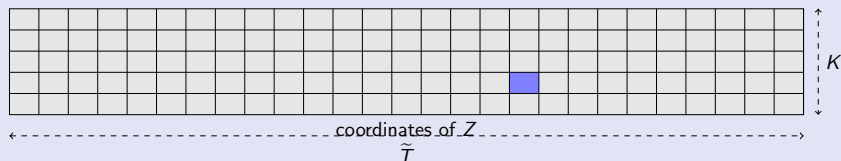
For each coordinate update, it is possible to maintain the value of β with $\mathcal{O}(KL)$ operations.

Z-step: Locally greedy coordinate descent (LGCD)

For the Greedy Coordinate Descent, only 1 coordinate is updated at each iteration: [\[Kavukcuoglu et al., 2010\]](#)

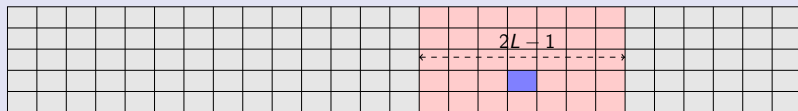
1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.
2. The updated coordinate is chosen
 - ▶ Cyclic selection: $\mathcal{O}(1)$ [\[Friedman et al., 2007\]](#)
 - ▶ Randomized selection: $\mathcal{O}(1)$ [\[Nesterov, 2010\]](#)
 - ▶ Greedy selection: $\mathcal{O}(K\tilde{T})$ [\[Osher and Li, 2009\]](#)
by maximizing $|z_k[t] - z'_k[t]|$

We introduced the LGCD method which is an extension of GCD.



GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

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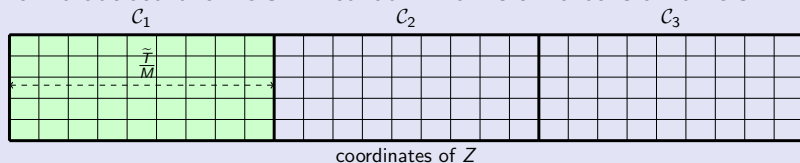


coordinates of Z

GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

But the update itself has complexity $\mathcal{O}(KL)$

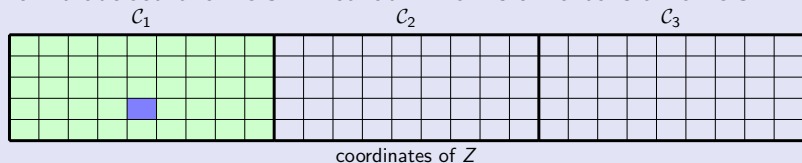
We introduced the LGCD method which is an extension of GCD.



With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}[$,

$$\mathcal{C}_m = [1, K] \times \left[\frac{(m-1)\tilde{T}}{M}, \frac{m\tilde{T}}{M} \right[$$

We introduced the LGCD method which is an extension of GCD.



With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}]$,

$$\mathcal{C}_m = [1, K] \times \left[\frac{(m-1)\tilde{T}}{M}, \frac{m\tilde{T}}{M} \right]$$

The coordinate to update is chosen greedily on a sub-domain \mathcal{C}_m

$$\frac{\tilde{T}}{M} = 2L - 1 \Rightarrow \mathcal{O}(\text{Coordinate selection}) = \mathcal{O}(\text{Coordinate Update})$$

The overall iteration complexity is $\mathcal{O}(KL)$ instead of $\mathcal{O}(K\tilde{T})$.

\Rightarrow Efficient for sparse Z

D-step: solving for the atoms

The dictionary update is performed by minimizing

$$\min_{\|D_k\|_2 \leq 1} E(D) \triangleq \sum_{n=1}^N \frac{1}{2} \|X^n - \sum_{k=1}^K z_k^n * D_k\|_2^2 . \quad (3)$$

Computing $\nabla_{d_k} E(\{d_k\}_k)$ can be done efficiently

$$\nabla_D E(D) = \sum_{n=1}^N (z_k^n)^\top * \left(x^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

\Rightarrow Solve with Projected Gradient Descent (PGD) with an Armijo backtracking line-search for the D-step [\[Wright and Nocedal, 1999\]](#).

D-step: solving for the atoms

We use the projected gradient descent with an Armijo backtracking line-search [Wright and Nocedal \[1999\]](#) for both u-step and v-step for

$$\min_{\substack{\|u_k\|_2 \leq 1 \\ \|v_k\|_2 \leq 1}} E(u_k, v_k) \triangleq \sum_{n=1}^N \frac{1}{2} \|X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top)\|_2^2 . \quad (4)$$

One important computation trick is for fast computation of the gradient.

$$\begin{aligned} \nabla_{u_k} E(u_k, v_k) &= \nabla_{D_k} E(u_k, v_k) v_k \in \mathbb{R}^P , \\ \nabla_{v_k} E(u_k, v_k) &= u_k^\top \nabla_{D_k} E(u_k, v_k) \in \mathbb{R}^L , \end{aligned}$$

Computing $\nabla_{D_k} E(u_k, v_k)$ can be done efficiently

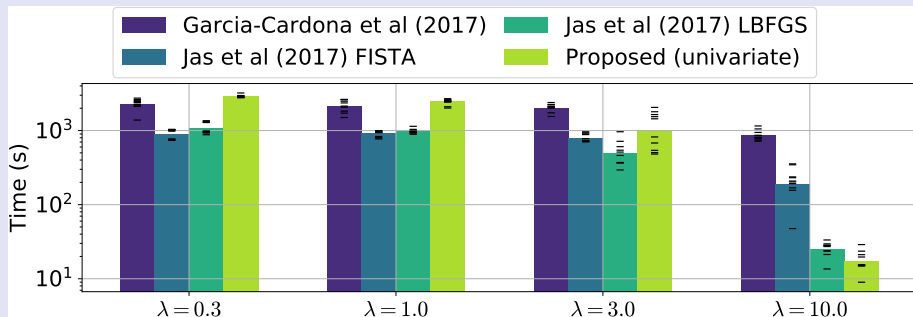
$$\nabla_{D_k} E(u_k, v_k) = \sum_{n=1}^N (z_k^n)^\top * \left(X^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

Experiments

Good time to wake-up if you got lost in the previous section!

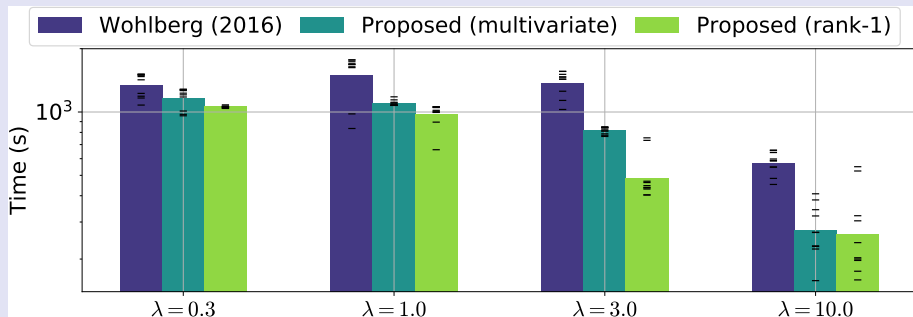
Fast optimization

Comparison with univariate methods on somato dataset with
 $T = 134,700$, $K = 8$ and $L = 128$



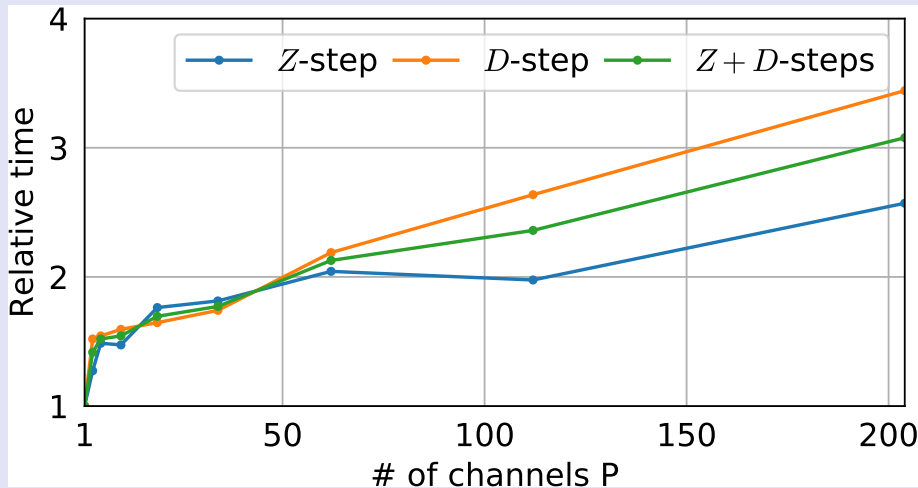
Fast optimization

Comparison with multivariate methods on somato dataset with $T = 134,700$, $K = 8$, $P = 5$ and $L = 128$



Good scaling in the number of channels P

Scaling relative to P on somato dataset with $T = 134,700$, $K = 2$, and $L = 128$



Test the pattern recovery capabilities of our method on simulated data,

$$X^n = \sum_{k=1}^2 z_k * (u_k v_k^\top) + \mathcal{E}$$

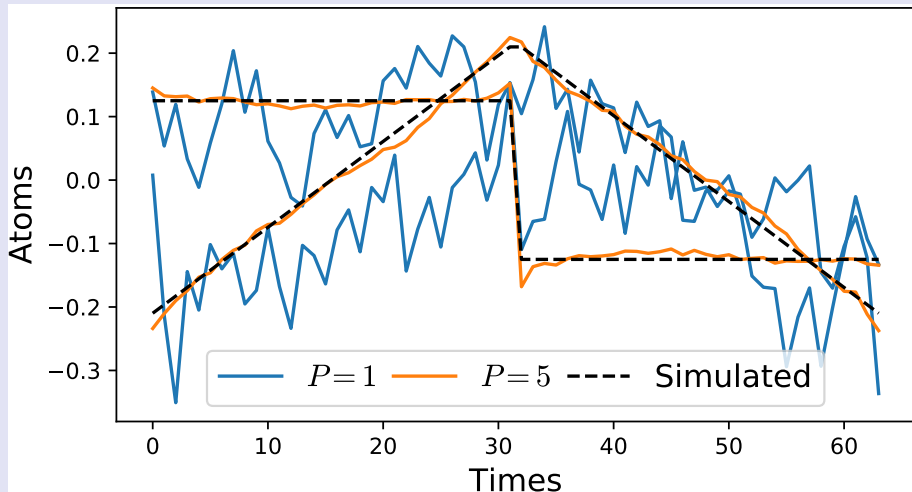
where (u_k, v_k) are chosen patterns of rank-1 and the activated coefficient $z_k^n[t]$ are drawn uniformly and their value are uniform in $[0, 1]$.

The noise \mathcal{E} is generated as a gaussian white noise with variance σ .

We set $N = 100$, $L = 64$ and $\tilde{T} = 640$

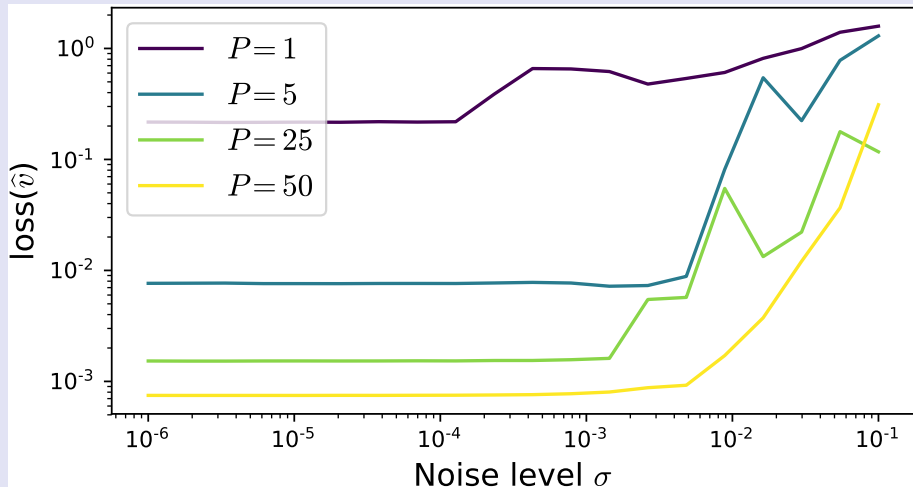
Pattern recovery

Patterns recovered with $P = 1$ and $P = 5$. The signals were generated with the two simulated temporal patterns and with $\sigma = 10^{-3}$.



Pattern recovery

Evolution of the recovery loss with σ for different values of P . Using more channels improves the recovery of the original patterns.

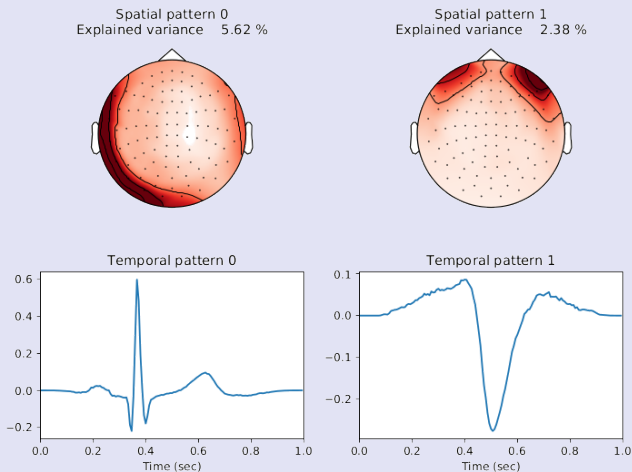


Experiments on MEG data

Even better time to wake-up!

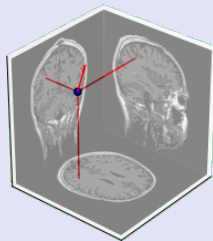
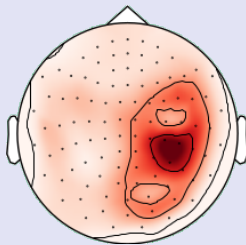
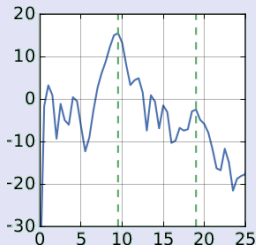
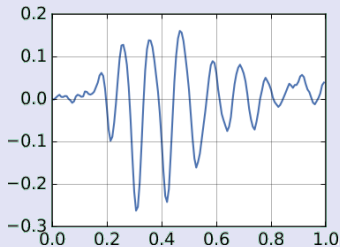
MNE somatosensory data

A selection of temporal waveforms of the atoms learned on the MNE sample dataset.



MNE somatosensory data

Atoms revealed using the MNE somatosensory data. Note the non-sinusoidal comb shape of the mu rhythm.



Conclusion

- ▶ We proposed a model for multivariate CSC with rank-1 constraint. This model makes sense for different type of data.
- ▶ We proposed a fast algorithm to solve the optimization problem involved in this model.
- ▶ We demonstrated numerically the performance of our algorithm on both simulated and real datasets.
- ▶ We illustrated the benefit of such method to study electromagnetic signals form recorded from brain activity.

DiCoDiLe: Distributed Convolutional Dictionary Learning

References

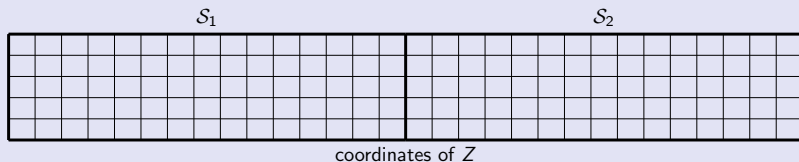
- ▶ Moreau, T., Oudre, L., and Vayatis, N. (2018). [DICOD: Distributed Convolutional Sparse Coding](#).
In *International Conference on Machine Learning (ICML)*, pages 3626–3634, Stockholm, Sweden. PMLR (80)
- ▶ Moreau, T. and Gramfort, A. (2019). [Distributed Convolutional Dictionary Learning \(DiCoDiLe\): Pattern Discovery in Large Images and Signals](#).
preprint ArXiv, 1901.09235

Weak dependence of the coordinate updates

The update of the W coordinates $(k_w, \omega_w)_{w=1}^W$ with additive update $\Delta Z_{k_w}[\omega_w]$ changes the cost by:

$$\Delta E = \underbrace{\sum_{i=1}^W \Delta E_w}_{\text{iterative steps}} - \underbrace{\sum_{w \neq w'} (d_{k_w} * d_{k_{w'}}^\dagger)[\omega_{w'} - \omega_w] \Delta Z_{k_w}[\omega_w] \Delta Z_{k_{w'}}[\omega_{w'}]}_{\text{interference}},$$

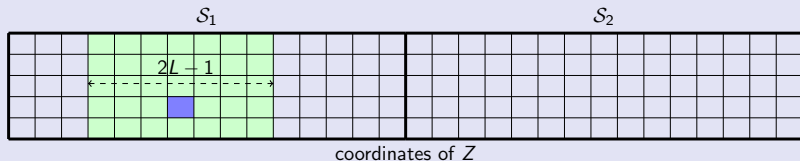
\Rightarrow If the updates are far enough, they can be considered as independent.



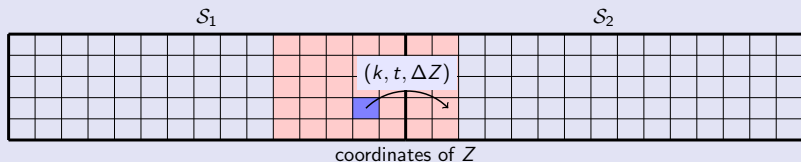
- Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.

DICOD: Distributed Convolutional Coordinate Descent

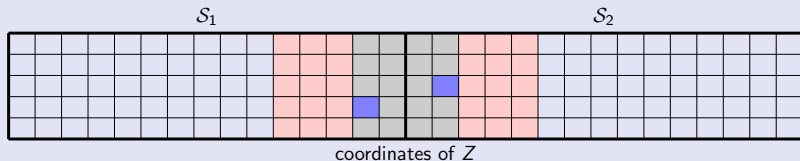
[Moreau et al., 2018]



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- ▶ Use CD updates in parallel in each sub-segment.



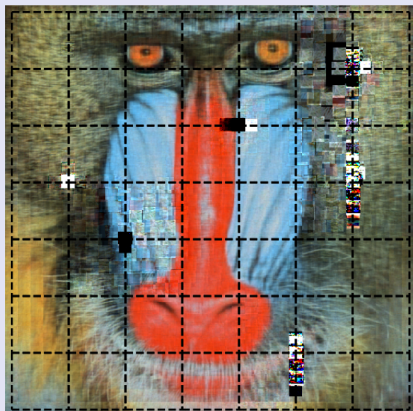
- Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- Use CD updates in parallel in each sub-segment.
- Notify neighbor workers when the update is on the border of \mathcal{S}_w .



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- ▶ Use CD updates in parallel in each sub-segment.
- ▶ Notify neighbor workers when the update is on the border of \mathcal{S}_w .
- ▶ What do we do when two updates are interfering?

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

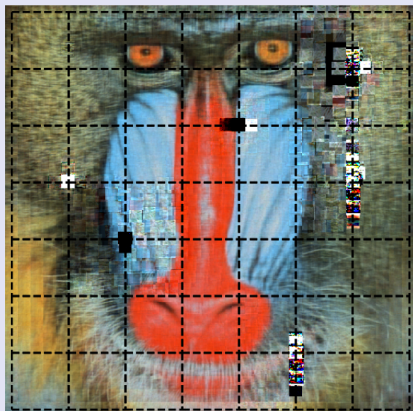
[Moreau and Gramfort, 2019]



- ▶ DICOD does not work for splits in dimension > 1 .

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

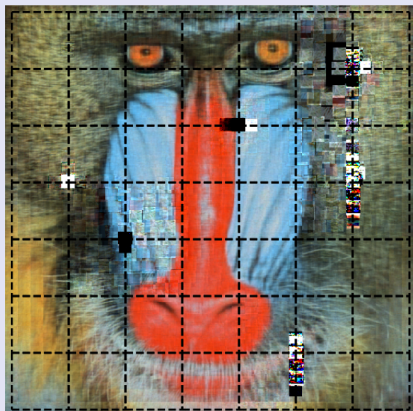
[Moreau and Gramfort, 2019]



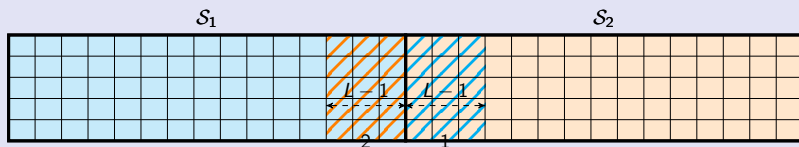
- ▶ DICOD does not work for splits in dimension > 1 .
- ▶ Extension require to control interferences.

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

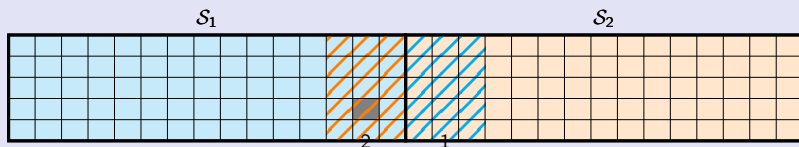
[Moreau and Gramfort, 2019]



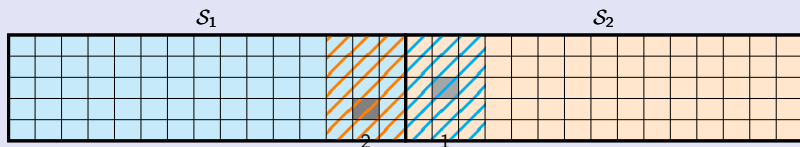
- ▶ DICOD does not work for splits in dimension > 1 .
- ▶ Extension require to control interferences.
- ▶ Use asynchronous mechanism: Soft-lock.



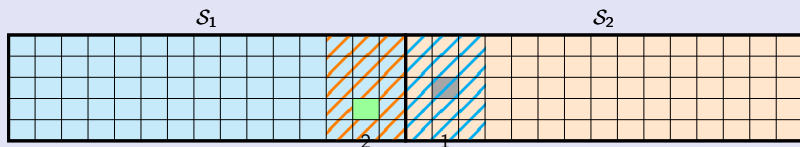
- Keep track of the value of the optimal update in an extended zone of size $L - 1$.



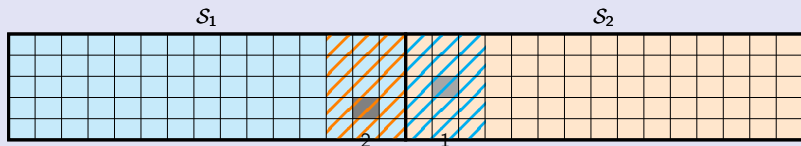
- Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- Select an update candidate with LGCD.



- Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- Select an update candidate with LGCD.
- If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.



- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.
- ▶ If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.
- ▶ Only perform the update if it is larger than the other update.



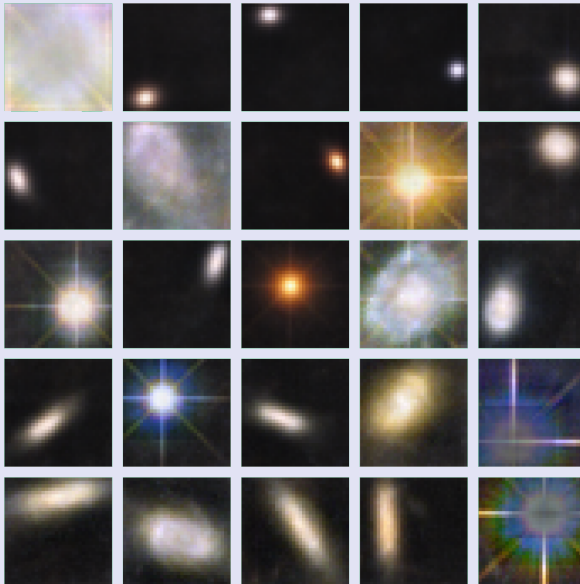
- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.
- ▶ If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.
- ▶ Only perform the update if it is larger than the other update.

⇒ Give an update order asynchronously.

Images from Hubble Space Telescope




Images from Hubble Space Telescope




Thanks for your attention!


Code available online:

 **alphacsc** : [alphacsc.github.io](https://github.com/alphacsc)

 **DiCoDiLe** : github.com/tommoral/dicodile

Slides are on my web page:

 tommoral.github.io

 [@tomamoral](https://twitter.com/tomamoral)

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