

Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals

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INRIA Saclay

Joint work with Dupré La Tour T., Mainak J., Gramfort A.



Goal: Study the brain mechanisms while it is functioning.

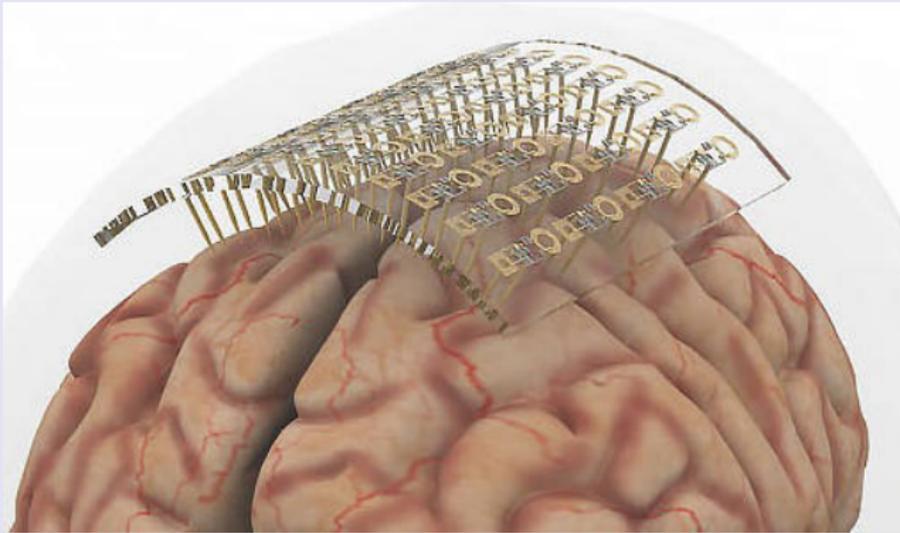
Outputs:

- ▶ **Functional Atlases:** Link areas of the brain to specific cognitive functions.
- ▶ **Functional Connectivity:** Highlight the information flow in the brain.
- ▶ **Healthcare:** Develop bio-markers for neurological disorders.
- ▶ ...

Context: Functional Neuroimaging

How to record living brains activity: **Electrophysiology**

Direct measurement of electrical activity.



High Localization

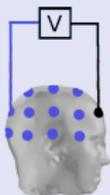
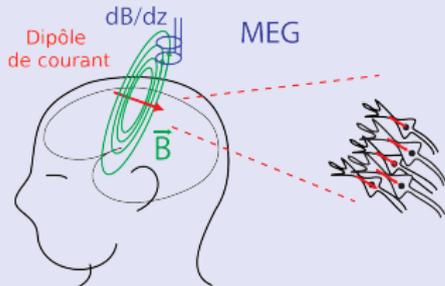
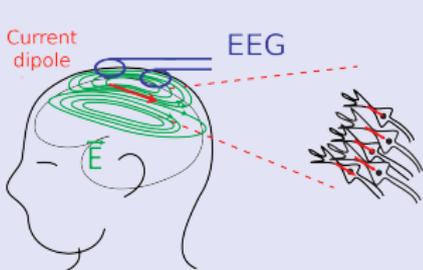
Low Resolution

Invasive

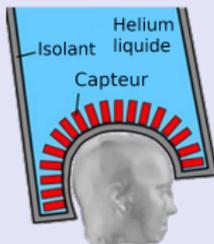
Context: functional Neuroimaging

How to record living brains activity: **Electrophysiology**

Remote measurement of the electrical activity.



No Localization

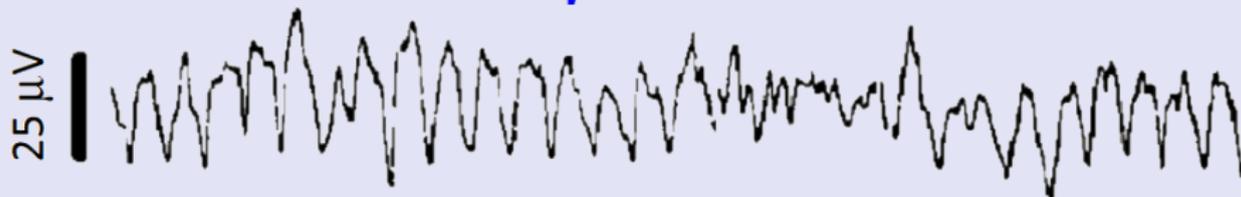


Global

Non Invasive

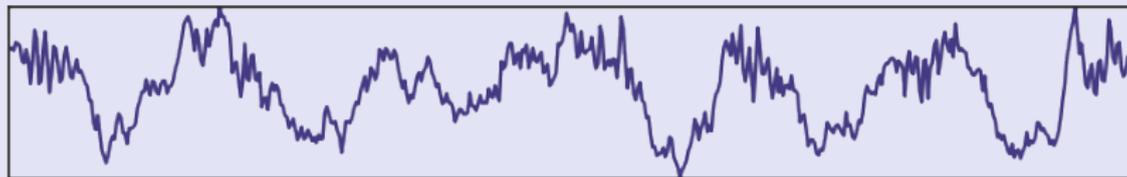
K-Complex

Sleep Spindle



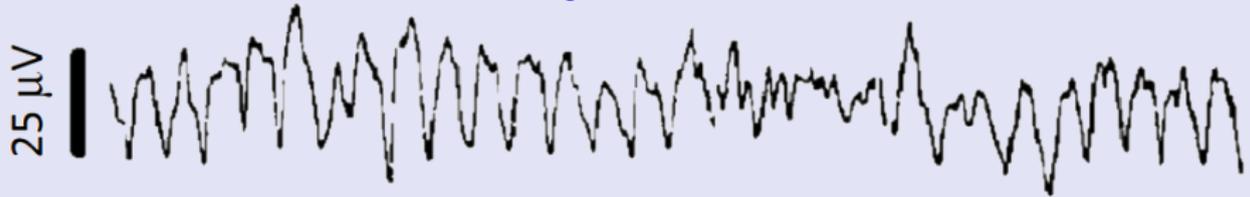
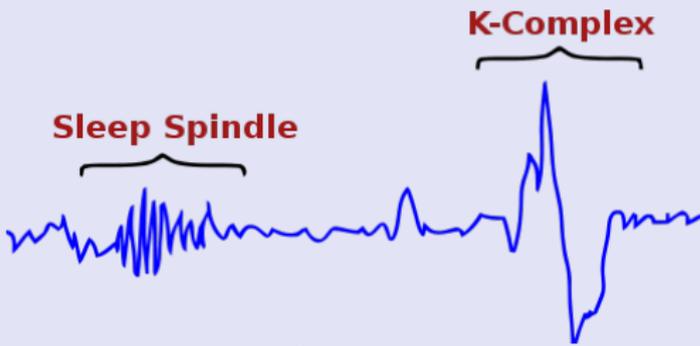
1 s

[S. Cole, B. Voytek (2017) Trends in Cognitive Sciences]



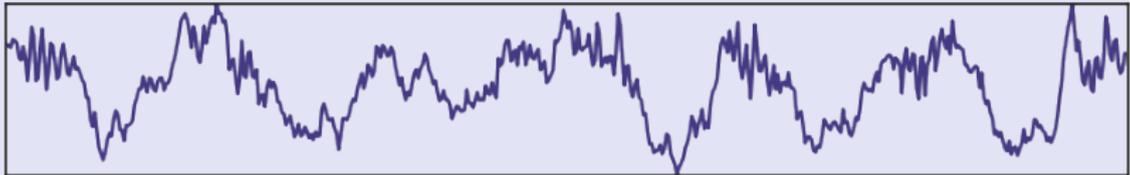
[Dupré la Tour, Tallot, Grabot, Doyère, van Wassenhove, Grenier, Gramfort (2017) PLOS Computational biology]

Neural signals
exhibit diverse and
complex
morphologies



1 s

[S. Cole, B. Voytek (2017) Trends in Cognitive Sciences]



[Dupré la Tour, Tallot, Grabot, Doyère, van Wassenhove, Grenier, Gramfort
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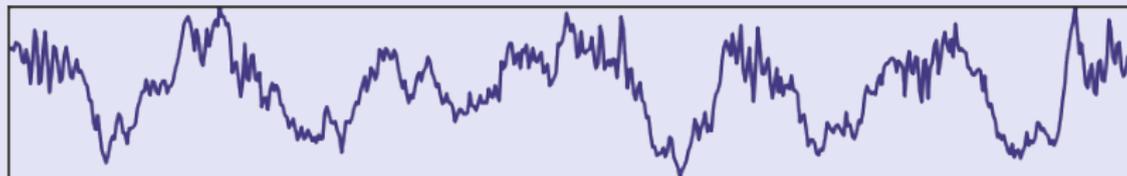
25 μ V

Waveform shape can be related to diseases
e.g. Parkinson

[Jackson et al. (2019)]

1 s

[S. Cole, B. Voytek (2017) Trends in Cognitive Sciences]



[Dupré la Tour, Tallot, Grabot, Doyère, van Wassenhove, Grenier, Gramfort (2017) PLOS Computational biology]

"Textbook" brain rhythm



Gamma
(< 25 Hz)



Beta
($12 - 25$ Hz)



Alpha
($8 - 12$ Hz)



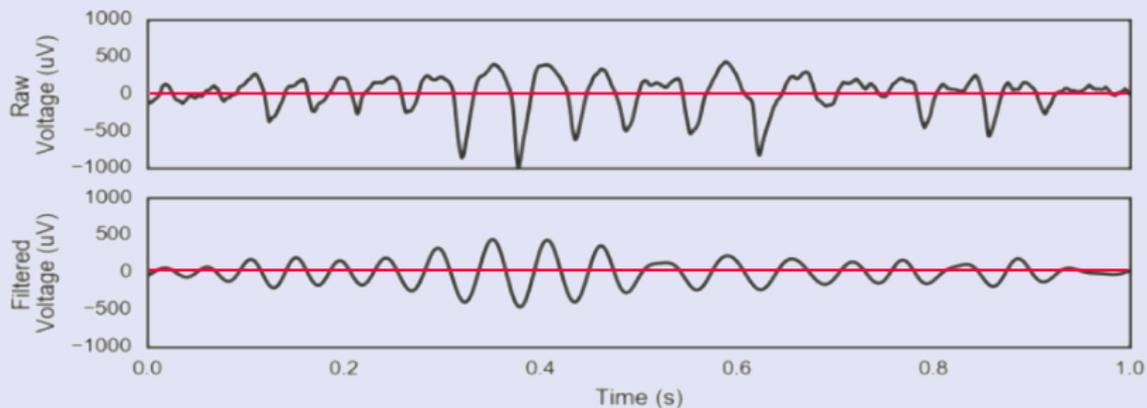
Theta
($8 - 12$ Hz)



Delta
($1 - 4$ Hz)

Linear filtering

After Linear filters, everything looks like a sinusoid.



⇒ Lose the asymmetry and the shape information.

Fourier Fallacy

” Even though it may be possible to analyze the complex forms of brain waves into a **number of different sine-wave** frequencies, this may lead only to what might be termed a “**Fourier fallacy**”, if one assumes **ad hoc** that all of the necessary frequencies actually occur as periodic phenomena in **cell groups** within the brain.”

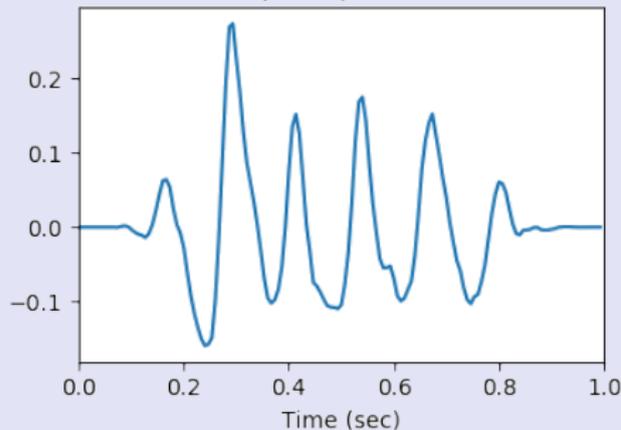
[Jasper (1948)]

Fourier Fallacy

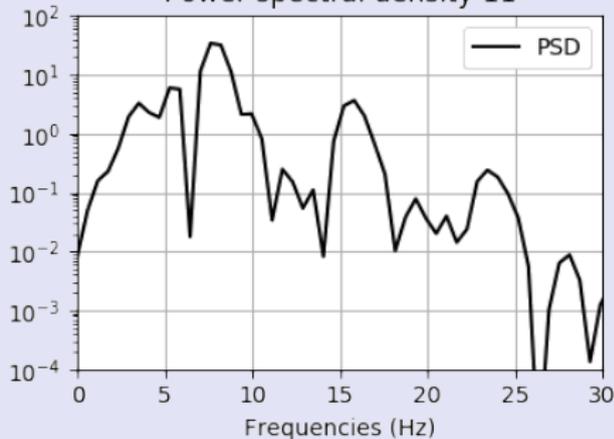
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[Jasper (1948)]

Temporal pattern 11



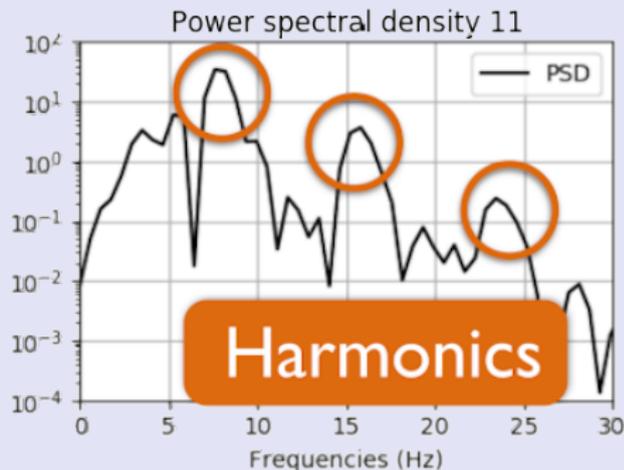
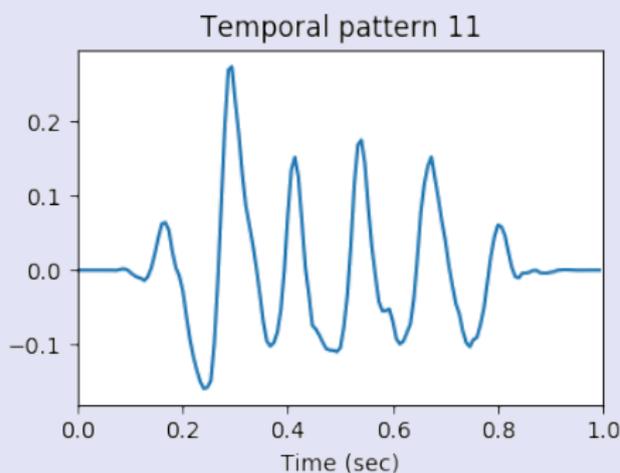
Power spectral density 11



Fourier Fallacy

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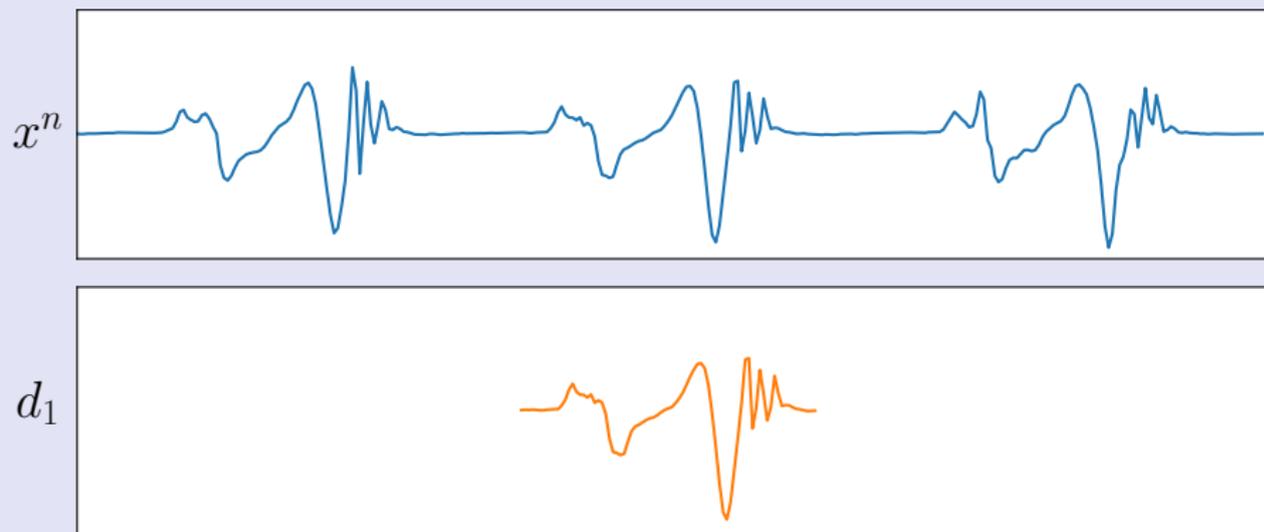


Learning the waveform: Convolutional Dictionary Learning

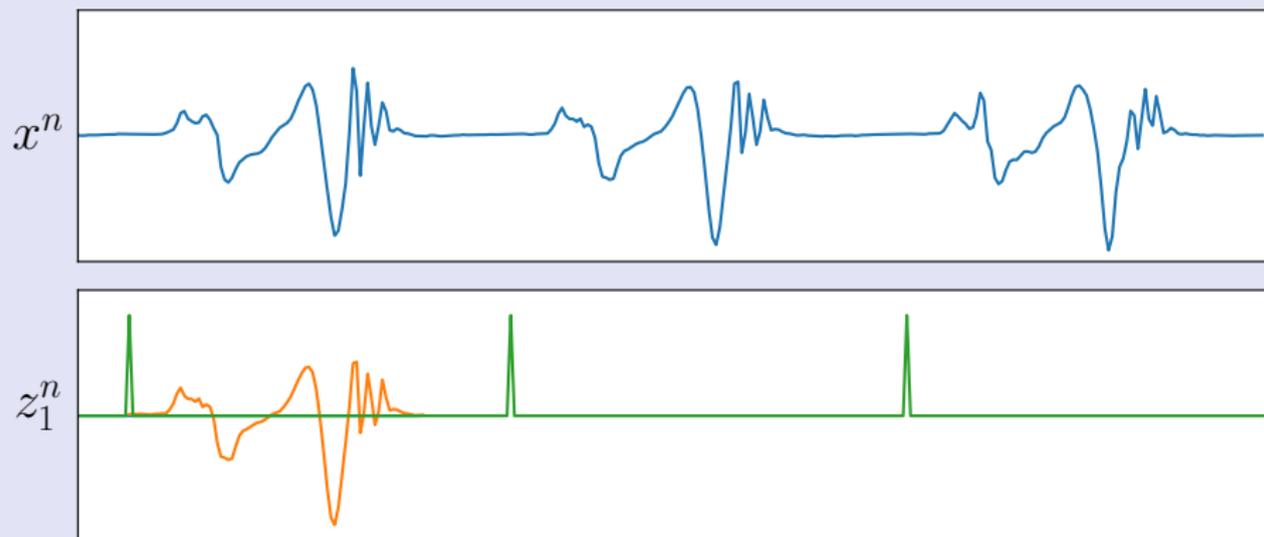
References

- ▶ Grosse, R., Raina, R., Kwong, H., and Ng, A. Y. (2007). [Shift-Invariant Sparse Coding for Audio Classification](#). *Cortex*, 8:9

Local structure in signals



Local structure in signals



Local structure in signals



Local structure in signals

Key idea: decouple the localization of the patterns and their shape



Local structure in signals

Key idea: decouple the localization of the patterns and their shape



Local structure in signals

Key idea: decouple the localization of the patterns and their shape



$$\boxed{x^n}[t] = \sum_{k=1}^K (\boxed{z_k^n} * \boxed{d_k})[t] + \varepsilon[t]$$

For a set of N univariate signals x^n , solve

$$\min_{d,z} \sum_{n=1}^N \frac{1}{2} \left\| x^n - \sum_{k=1}^K z_k^n * d_k \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1,$$

$$\text{s.t.} \quad \|d_k\|_2^2 \leq 1$$

Hypothesis: patterns d_k are not present everywhere in the signal. They are localized in time.

⇒ Sparse activation signals z

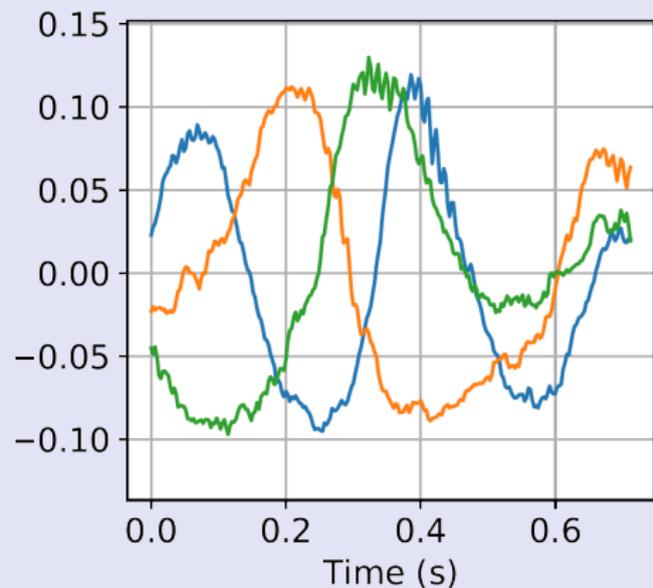
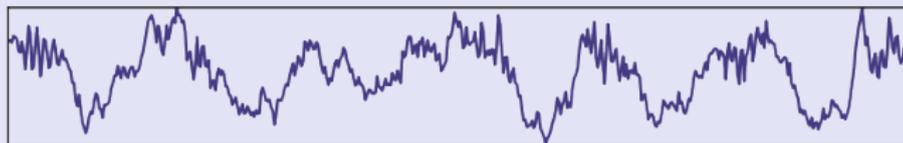
Technical hypothesis: the patterns are in the ℓ_2 -ball: $\|d_k\|_2^2 \leq 1$.

Bi-convex: The problem is not jointly convex in z_k^n , and d_k but it is convex in each block of coordinate.

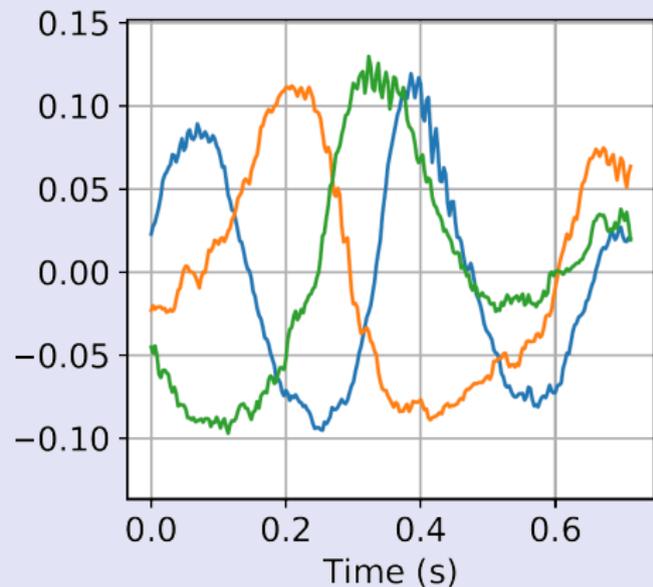
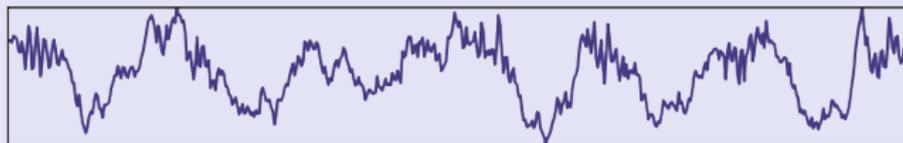
Alternate minimization (*a.k.a.* Bloc Coordinate Descent):

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal x^n .
- ▶ **D-step:** given a fixed estimate of the activation, update the atoms in the dictionary d_k .

Data:



Data:



What to do
in the case of
multivariate
signals?

How to extend CSC to multivariate signals?

We can just use multivariate convolution,

$$\underbrace{X[t]}_{\in \mathbb{R}^P} = \sum_{k=1}^K (z_k * D_k) [t] = \sum_{k=1}^K \sum_{\tau=1}^L z_k[t - \tau] \underbrace{D_k[\tau]}_{\in \mathbb{R}^P}$$

with:

- ▶ X a multivariate signal of length T in \mathbb{R}^P
- ▶ D_k a multivariate signal of length L in \mathbb{R}^P
- ▶ z_k a univariate activation signal of length $\tilde{T} = T - L + 1$

However, this model does not account for the physics of the problem.

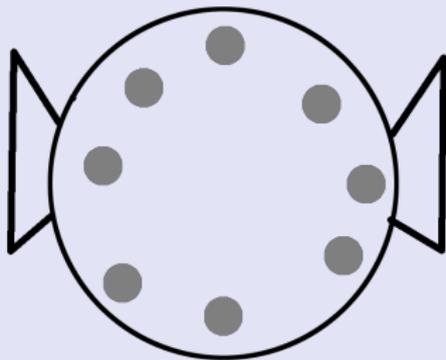
Rank-1 constrained dictionary learning

References

- ▶ Dupré la Tour, T., Moreau, T., Jas, M., and Gramfort, A. (2018).
Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals.
In *Advances in Neural Information Processing Systems (NeurIPS)*, pages
3296–3306, Montreal, Canada

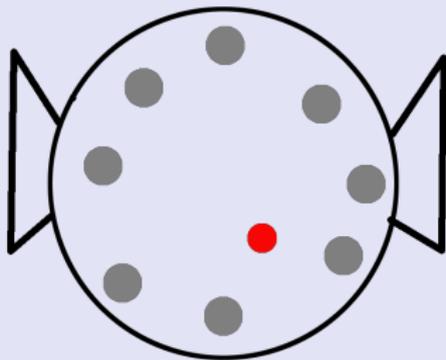
EM wave diffusion

- ▶ Recording here with 8 sensors



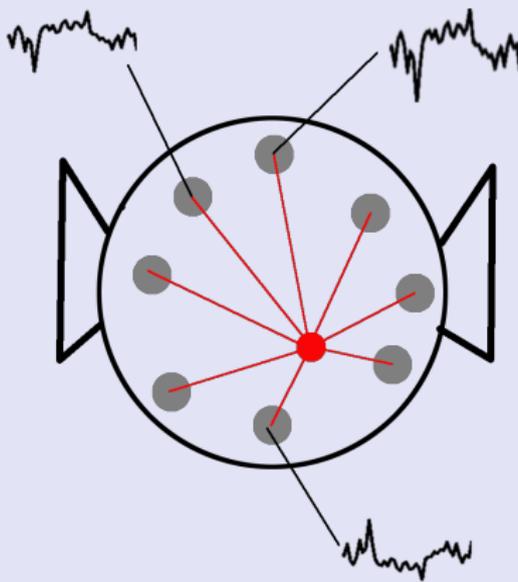
EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain



EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain
- ▶ The electric field is spread **linearly** and **instantaneously** over all sensors (Maxwell equations)



Multivariate CSC with rank-1 constraint

Idea: Impose a rank-1 constraint on the dictionary atoms D_k

To make the problem tractable, we decided to use auxiliary variables u_k and v_k s.t. $D_k = u_k v_k^\top$.

$$\begin{aligned} \min_{u_k, v_k, z_k^n} \sum_{n=1}^N \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top) \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1, \\ \text{s.t. } \|u_k\|_2^2 \leq 1, \|v_k\|_2^2 \leq 1 \text{ and } z_k^n \geq 0. \end{aligned} \quad (1)$$

Here,

- ▶ $u_k \in \mathbb{R}^P$ is the spatial pattern of our atom
- ▶ $v_k \in \mathbb{R}^L$ is the temporal pattern of our atom

Tri-convex: The problem is not jointly convex in z_k^n , u_k and v_k but it is convex in each block of coordinate.

We can use a block coordinate descent, aka alternate minimization, to converge to a local minima of this problem. The 3 following steps are applied alternatively:

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal X^n .
- ▶ **u-step:** given a fixed estimate of the activation and temporal pattern, update the spatial pattern u_k .
- ▶ **v-step:** given a fixed estimate of the activation and spatial pattern, update the temporal pattern v_k .

Z-step: Locally greedy coordinate descent (LGCD)

N independent problem such that

$$\min_{z_k^n \geq 0} \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * D_k \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1 .$$

This problem is convex in z_k and can be solved with different techniques:

- ▶ Greedy CD [Kavukcuoglu et al., 2010]
- ▶ Fista [Chalasan et al., 2013]
- ▶ ADMM [Bristow et al., 2013]
- ▶ L-BFGS [Jas et al., 2017]

⇒ These methods can be slow for long signals as the complexity of each iteration is at least linear in the length of the signal.

Z-step: Locally greedy coordinate descent (LGCD)

For the Greedy Coordinate Descent, only 1 coordinate is updated at each iteration: [\[Kavukcuoglu et al., 2010\]](#)

1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.

$$z'_k[t] = \max \left(\frac{\beta_k[t] - \lambda}{\|D_k\|_2^2}, 0 \right),$$

$$\text{with } \beta_k[t] = \left[D_k^\top * \left(X - \sum_{l=1}^K z_l * D_l + z_k[t] e_t * D_k \right) \right] [t]$$

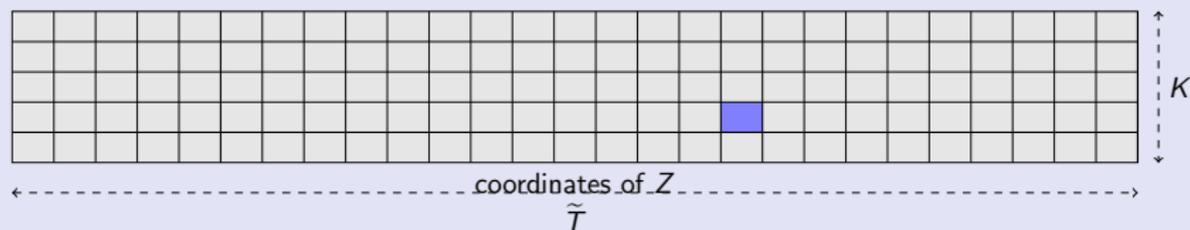
For each coordinate update, it is possible to maintain the value of β with $\mathcal{O}(KL)$ operations.

Z-step: Locally greedy coordinate descent (LGCD)

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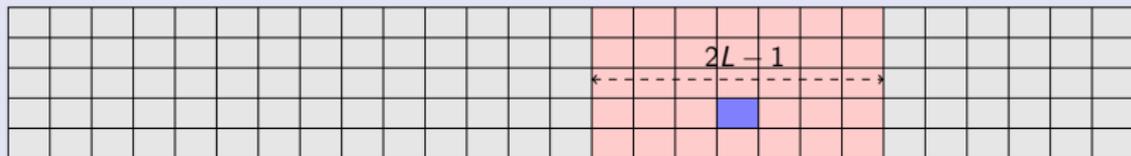
1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.
2. The updated coordinate is chosen
 - ▶ Cyclic selection: $\mathcal{O}(1)$ [\[Friedman et al., 2007\]](#)
 - ▶ Randomized selection: $\mathcal{O}(1)$ [\[Nesterov, 2010\]](#)
 - ▶ Greedy selection: $\mathcal{O}(K\tilde{T})$ [\[Osher and Li, 2009\]](#)
by maximizing $|z_k[t] - z'_k[t]|$

We introduced the LGCD method which is an extension of GCD.



GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

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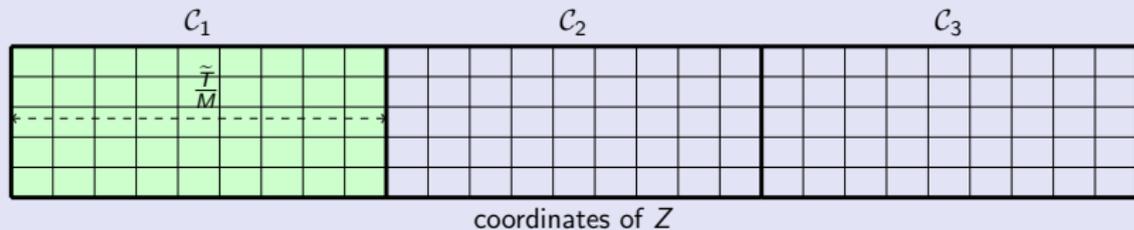


coordinates of Z

GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

But the update itself has complexity $\mathcal{O}(KL)$

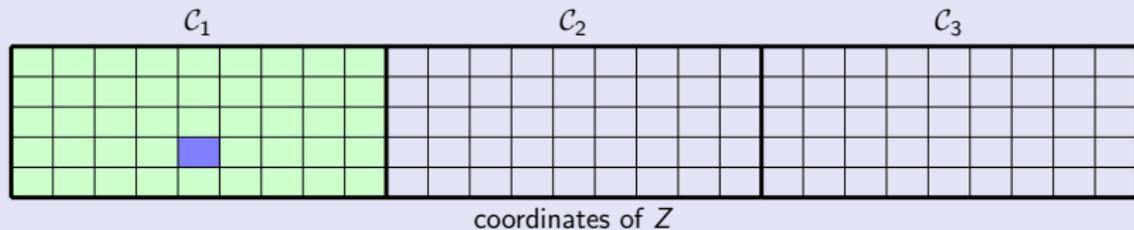
We introduced the LGCD method which is an extension of GCD.



With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}[$,

$$\mathcal{C}_m = [1, K] \times \left[\frac{(m-1)\tilde{T}}{M}, \frac{m\tilde{T}}{M} [$$

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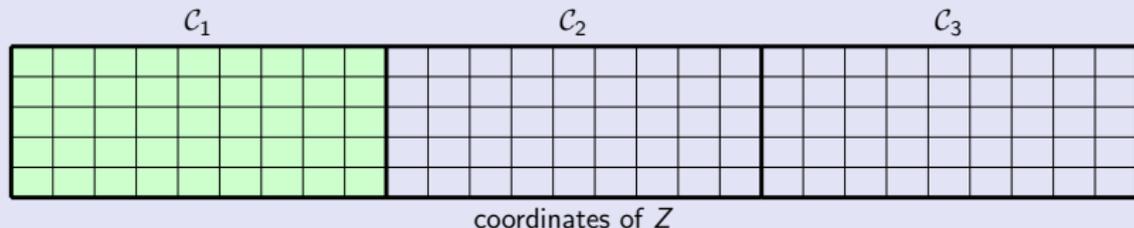
The coordinate to update is chosen greedily on a sub-domain \mathcal{C}_m

$$\frac{\tilde{T}}{M} = 2L - 1 \Rightarrow \mathcal{O}(\text{Coordinate selection}) = \mathcal{O}(\text{Coordinate Update})$$

The overall iteration complexity is $\mathcal{O}(KL)$ instead of $\mathcal{O}(K\tilde{T})$.

\Rightarrow Efficient for sparse Z

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With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}[$,

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The overall iteration complexity is $\mathcal{O}(KL)$ instead of $\mathcal{O}(K\tilde{T})$.

\Rightarrow Efficient for sparse Z

\Rightarrow Can be efficiently parallelized.

D-step: solving for the atoms

The dictionary update is performed by minimizing

$$\min_{\|D_k\|_2 \leq 1} E(D) \triangleq \sum_{n=1}^N \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * D_k \right\|_2^2 . \quad (2)$$

Computing $\nabla_{d_k} E(\{d_k\}_k)$ can be done efficiently

$$\nabla_D E(D) = \sum_{n=1}^N (z_k^n)^\top * \left(x^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

⇒ Solve with Projected Gradient Descent (PGD) with an Armijo backtracking line-search for the D-step [\[Wright and Nocedal, 1999\]](#).

D-step: solving for the atoms

We use the projected gradient descent with an Armijo backtracking line-search [Wright and Nocedal \[1999\]](#) for both u-step and v-step for

$$\min_{\substack{\|u_k\|_2 \leq 1 \\ \|v_k\|_2 \leq 1}} E(u_k, v_k) \triangleq \sum_{n=1}^N \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top) \right\|_2^2 . \quad (3)$$

One important computation trick is for fast computation of the gradient.

$$\begin{aligned} \nabla_{u_k} E(u_k, v_k) &= \nabla_{D_k} E(u_k, v_k) v_k \in \mathbb{R}^P, \\ \nabla_{v_k} E(u_k, v_k) &= u_k^\top \nabla_{D_k} E(u_k, v_k) \in \mathbb{R}^L, \end{aligned}$$

Computing $\nabla_{D_k} E(u_k, v_k)$ can be done efficiently

$$\nabla_{D_k} E(u_k, v_k) = \sum_{n=1}^N (z_k^n)^\dagger * \left(X^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

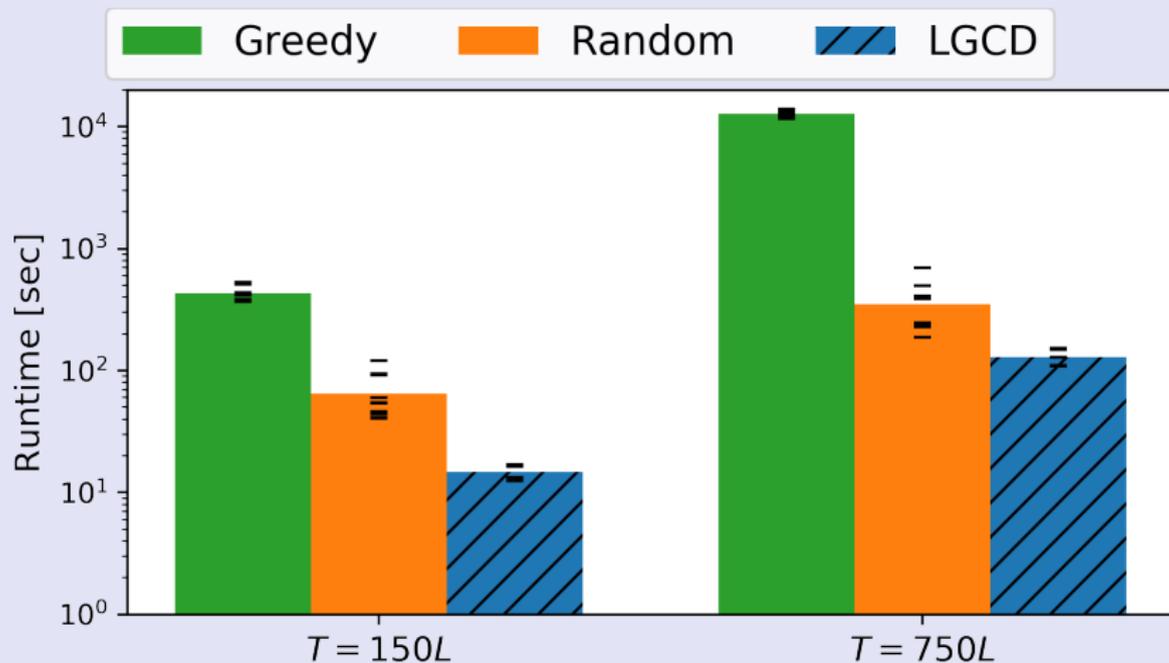
Experiments

Good time to wake-up if you got lost in the previous section!

Fast optimization

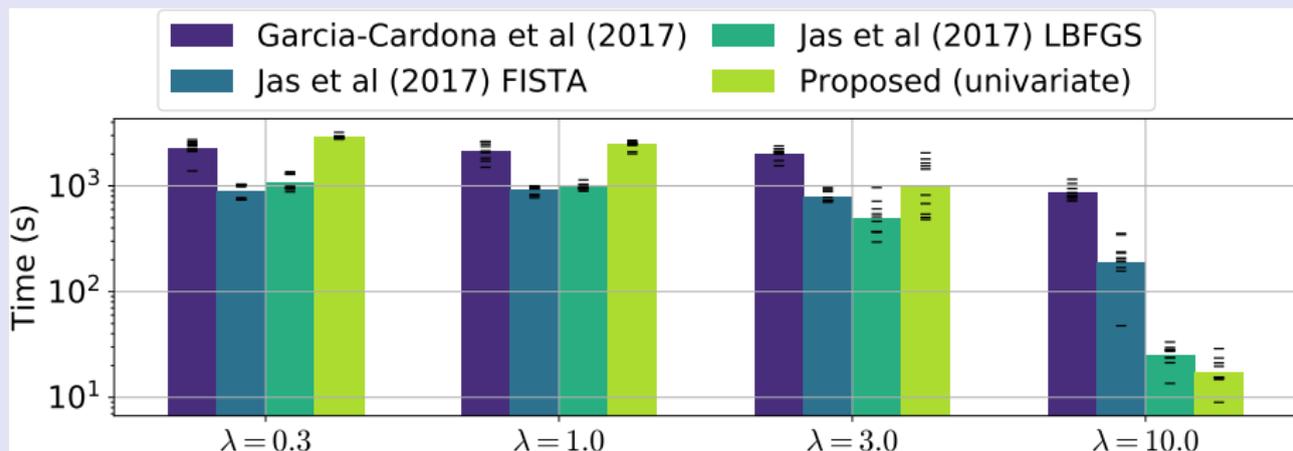
Comparison of the coordinate selection strategy for CD on simulated signals

We set $K = 10$, $L = 150$, $\lambda = 0.1\lambda_{\max}$



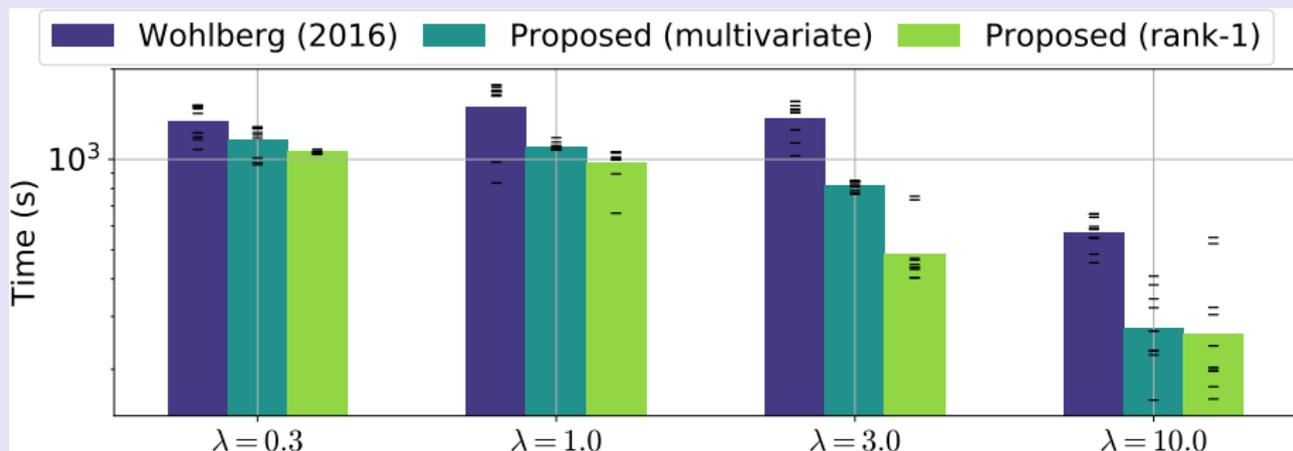
Fast optimization

Comparison with univariate methods on somato dataset with
 $T = 134,700$, $K = 8$ and $L = 128$



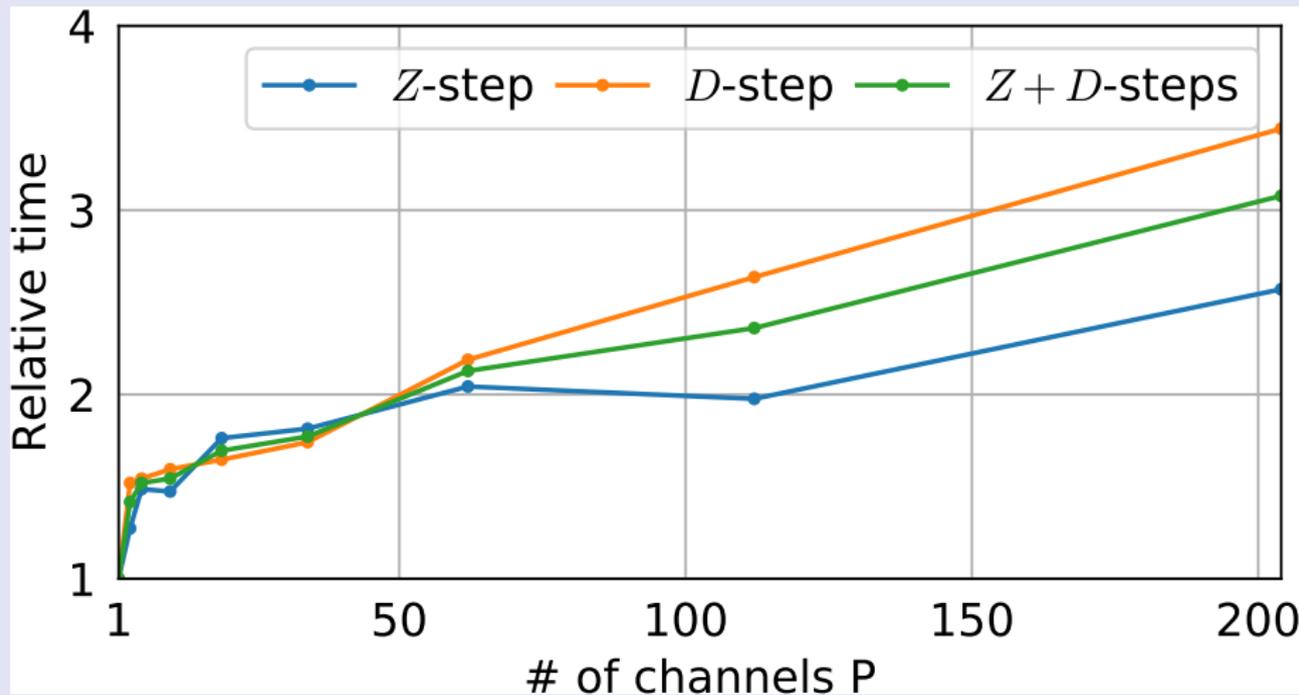
Fast optimization

Comparison with multivariate methods on somato dataset with $T = 134,700$, $K = 8$, $P = 5$ and $L = 128$



Good scaling in the number of channels P

Scaling relative to P on somato dataset with $T = 134,700$, $K = 2$, and $L = 128$



Test the pattern recovery capabilities of our method on simulated data,

$$X^n = \sum_{k=1}^2 z_k * (u_k v_k^\top) + \mathcal{E}$$

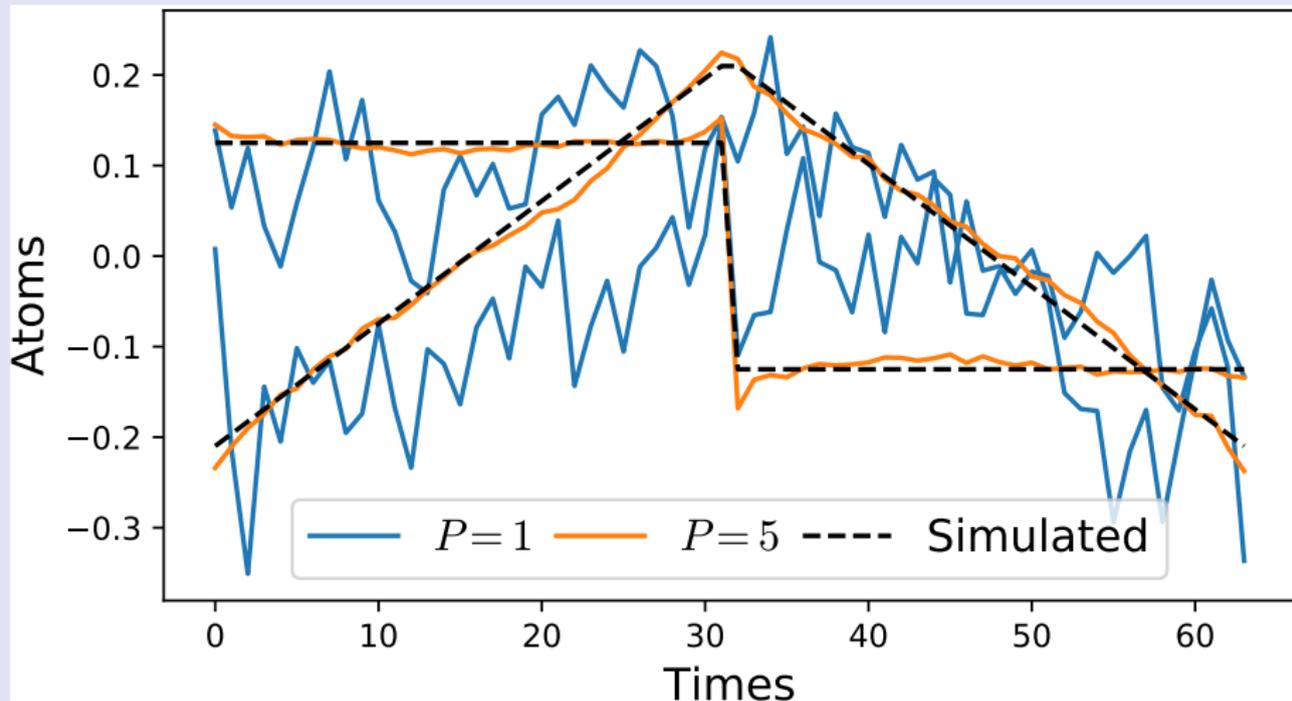
where (u_k, v_k) are chosen patterns of rank-1 and the activated coefficient $z_k^n[t]$ are drawn uniformly and their value are uniform in $[0, 1]$.

The noise \mathcal{E} is generated as a gaussian white noise with variance σ .

We set $N = 100$, $L = 64$ and $\tilde{T} = 640$

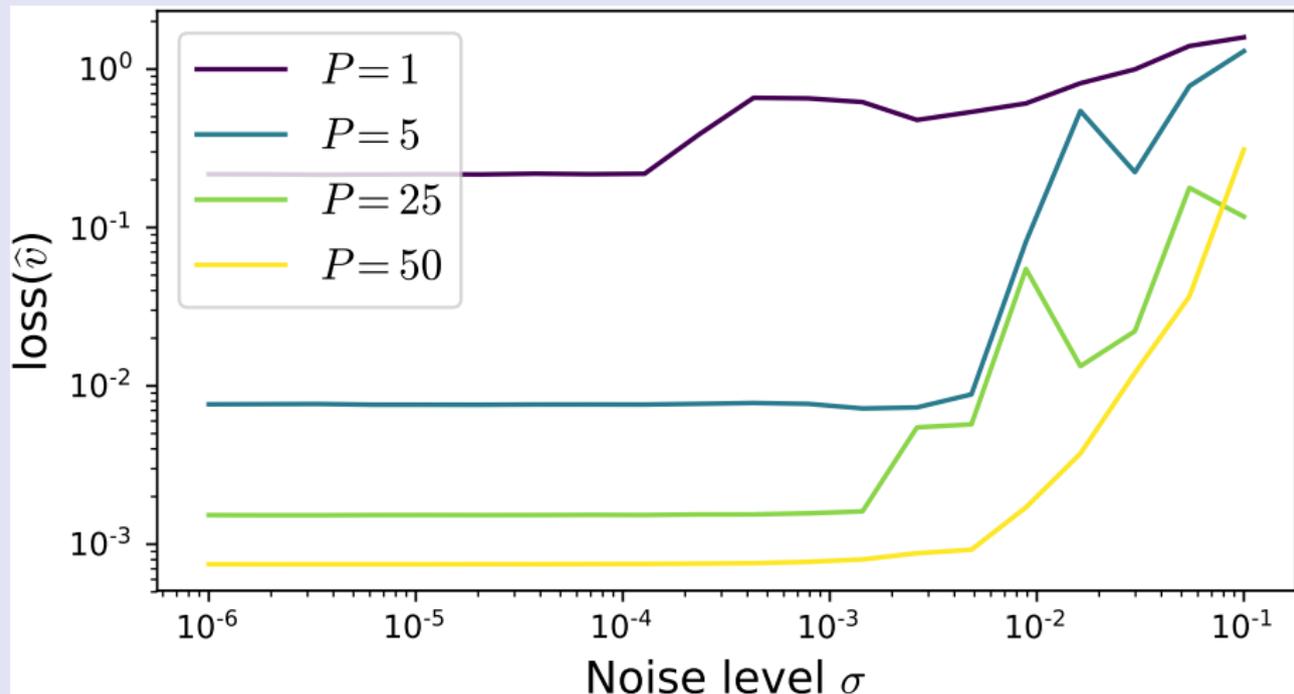
Pattern recovery

Patterns recovered with $P = 1$ and $P = 5$. The signals were generated with the two simulated temporal patterns and with $\sigma = 10^{-3}$.



Pattern recovery

Evolution of the recovery loss with σ for different values of P . Using more channels improves the recovery of the original patterns.



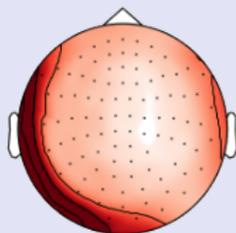
Experiments on MEG data

Even better time to wake-up!

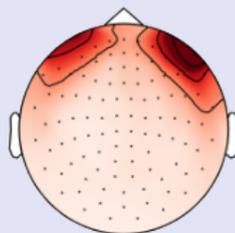
MNE somatosensory data

A selection of temporal waveforms of the atoms learned on the MNE sample dataset.

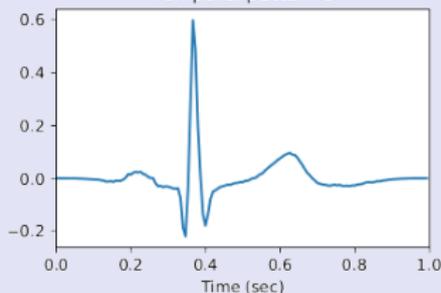
Spatial pattern 0
Explained variance 5.62 %



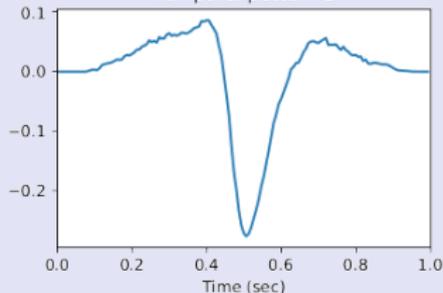
Spatial pattern 1
Explained variance 2.38 %



Temporal pattern 0

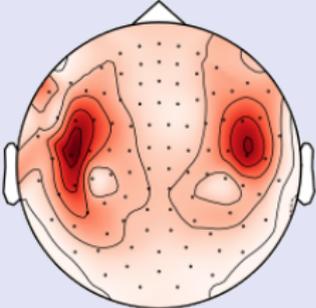


Temporal pattern 1

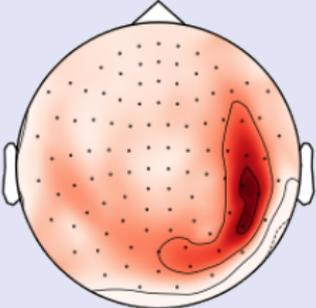


Learned atoms – Evoked response

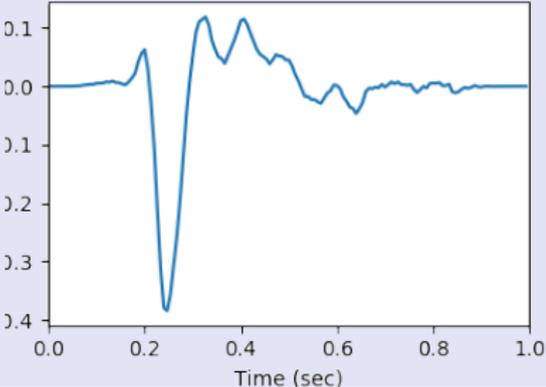
Spatial pattern 3



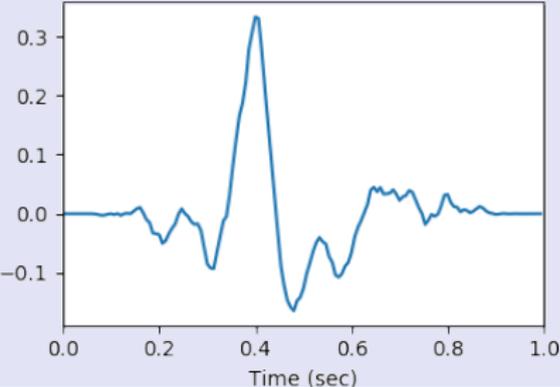
Spatial pattern 15



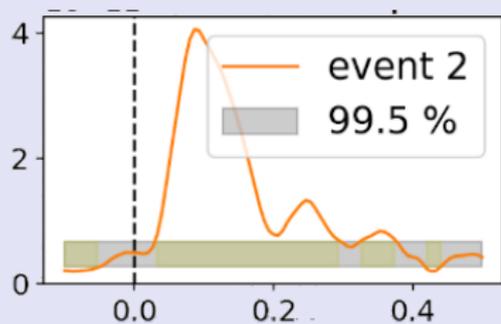
Temporal pattern 3



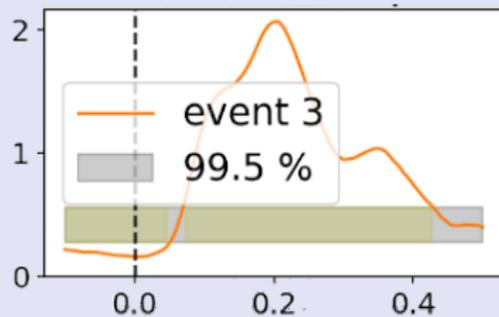
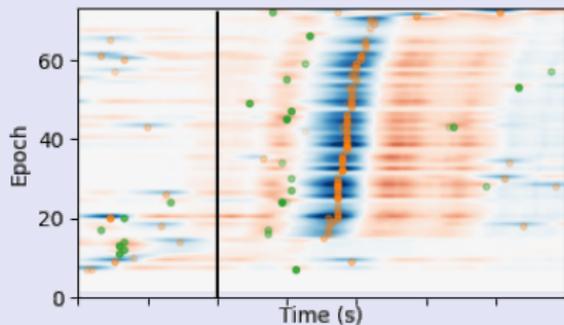
Temporal pattern 15



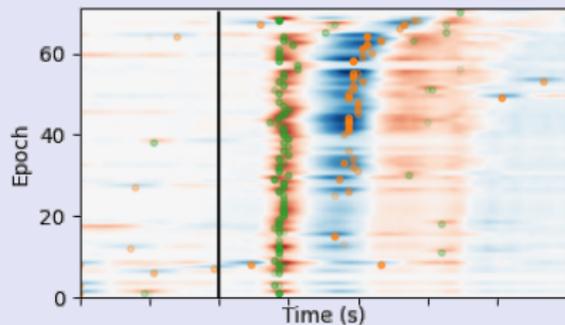
Learned atoms – Evoked response



Event 3 - 2-atoms



Event 4 - 2-atoms

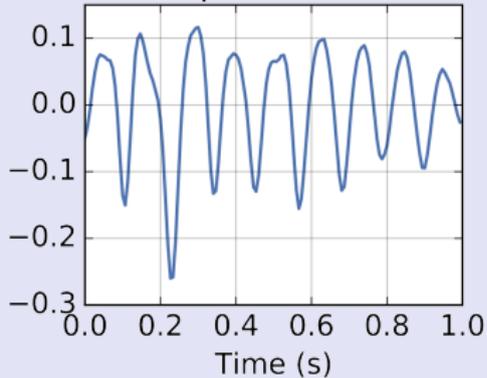


Learned atoms – Evoked response

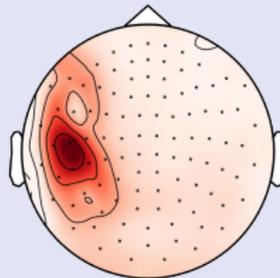


Learned atoms – Complex waveforms

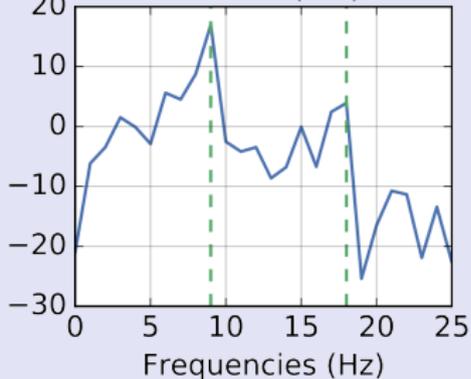
A. Temporal waveform



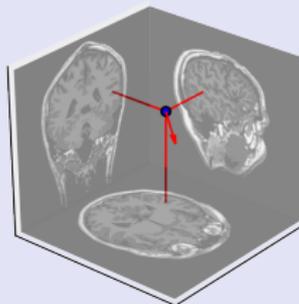
B. Spatial pattern



C. PSD (dB)



D. Dipole fit



alphaCSC: Convolution sparse coding for time-series

build passing  codecov 82%

This is a library to perform shift-invariant **sparse dictionary learning**, also known as time-series data. It includes a number of different models:

1. univariate CSC
2. multivariate CSC
3. multivariate CSC with a rank-1 constraint ^[1]
4. univariate CSC with an alpha-stable distribution ^[2]

A mathematical descriptions of these models is available [in the documentation](#).

Installation

To install this package, the easiest way is using `pip`. It will install this package and depends on `numpy` and `cython` for the installation so it is advised to install them please run one of the two commands:

(Latest stable version)

```
pip install numpy cython
pip install alphacsc
```

Python code online:
<https://alphacsc.github.io>

```
pip install alphacsc
```

Examples reproduce figures
from this talk!

Thanks for your attention!

Code available online:

 **alphacsc** : [alphacsc.github.io](https://github.com/alphacsc)

 **DiCoDiLe** : github.com/tommoral/dicodile

Slides are on my web page:

 tommoral.github.io

 [@tomamoral](https://twitter.com/tomamoral)